

# Monte Carlo Tutorial

## - a hands-on 4 week course

- Outline:
  - Lecture: Introduction to MC methods
  - Lecture: Practical MC
  - Exercises set 1: FLUKA basics
  - Exercises set 2: Advanced FLUKA
  - Exercises set 3: SHIELD-HIT12A basics
  - Exercises set 4: Catch-up, SHIELD-HIT12A + TRiP98

### Requirements:

- Laptop (ideally with some Linux distribution) registered on network
- Plotting capabilities (*use your own favourite tool, this is course is not about data processing* :)

# Monte Carlo Tutorial

## Part 1 - Introduction to Monte Carlo Methods

*IFJ-PAN, Cracow, May 2014*

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Dept. Physics and Astronomy  
Aarhus University, Denmark

# Treatment Planning

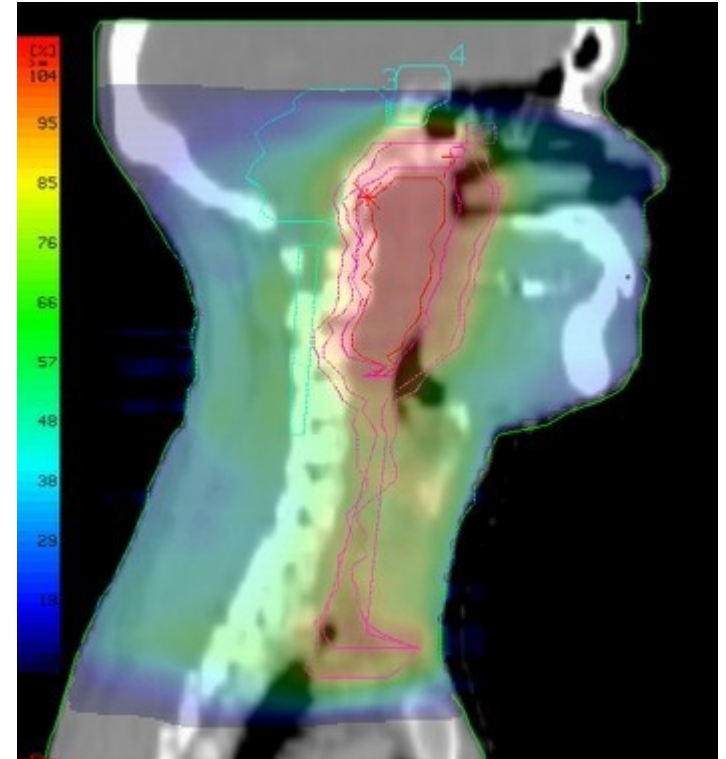
Radiation transport equation (see below) can **only** be solved analytically for **simple geometries** (paper+pencil method)

A treatment plan is not a simple geometry.

Photon, electron and ion calculation algorithms are mostly based on simple superposition of **pre-calculated dose kernels**.

Problems:

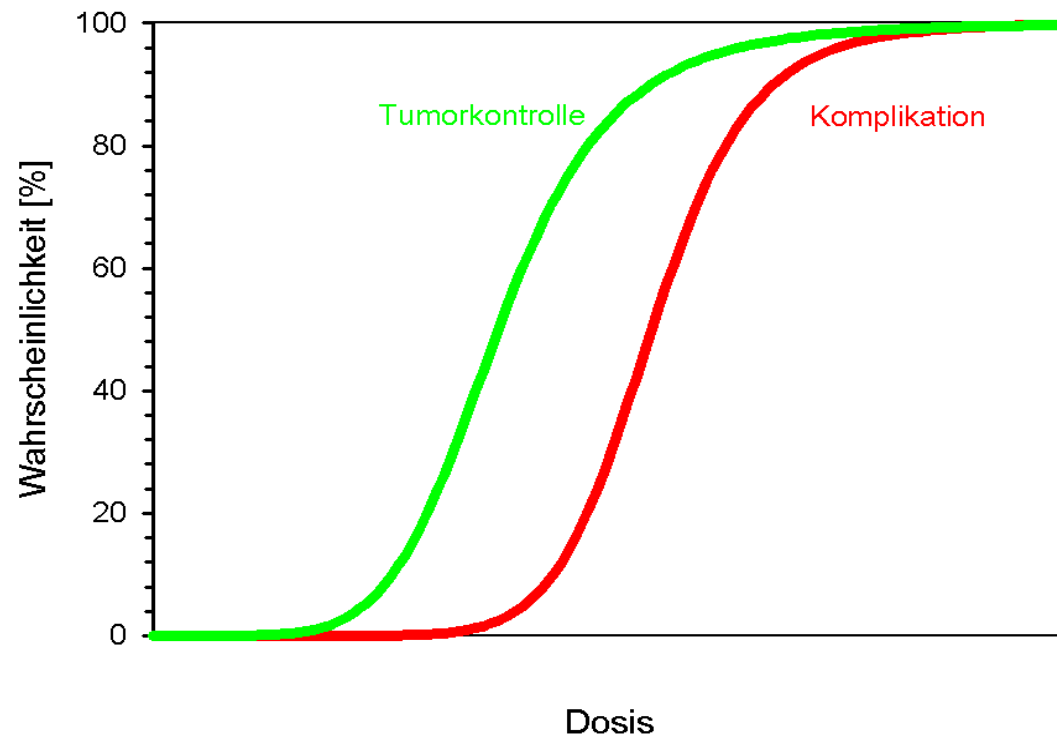
- Dose at **steep density gradients** are not well simulated, due to incorrect treatment of scattering (air cavities, metal implants)
- Dose to water is calculated, which is different from the actual **dose to medium**
- Some algorithms fail when (T)CPE cannot be applied



$$\nabla \cdot \vec{\Phi} = \text{net flow out}$$

$$\nabla \cdot \vec{\Phi} = - \int_{4\pi} d\Omega \int_{T_{cut}}^{\infty} dT \mu(T, \vec{\Omega}) \Phi_{T, \Omega} + \int_{4\pi} d\Omega \int_{T_{cut}}^{\infty} dT \int_{4\pi} d\Omega' \int_{T_{cut}}^{\infty} dT' \mu_{T, \Omega}(T', \Omega'; T, \Omega) \Phi_{T', \Omega'} + \int_{4\pi} d\Omega \int_{T_{cut}}^{\infty} dTS_{T, \Omega}$$

# The need for Precision and Accuracy

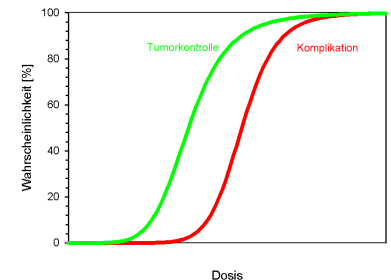


**TCP = Tumour Control Probability**

**NTCP = Normal Tissue  
Complication Probability**

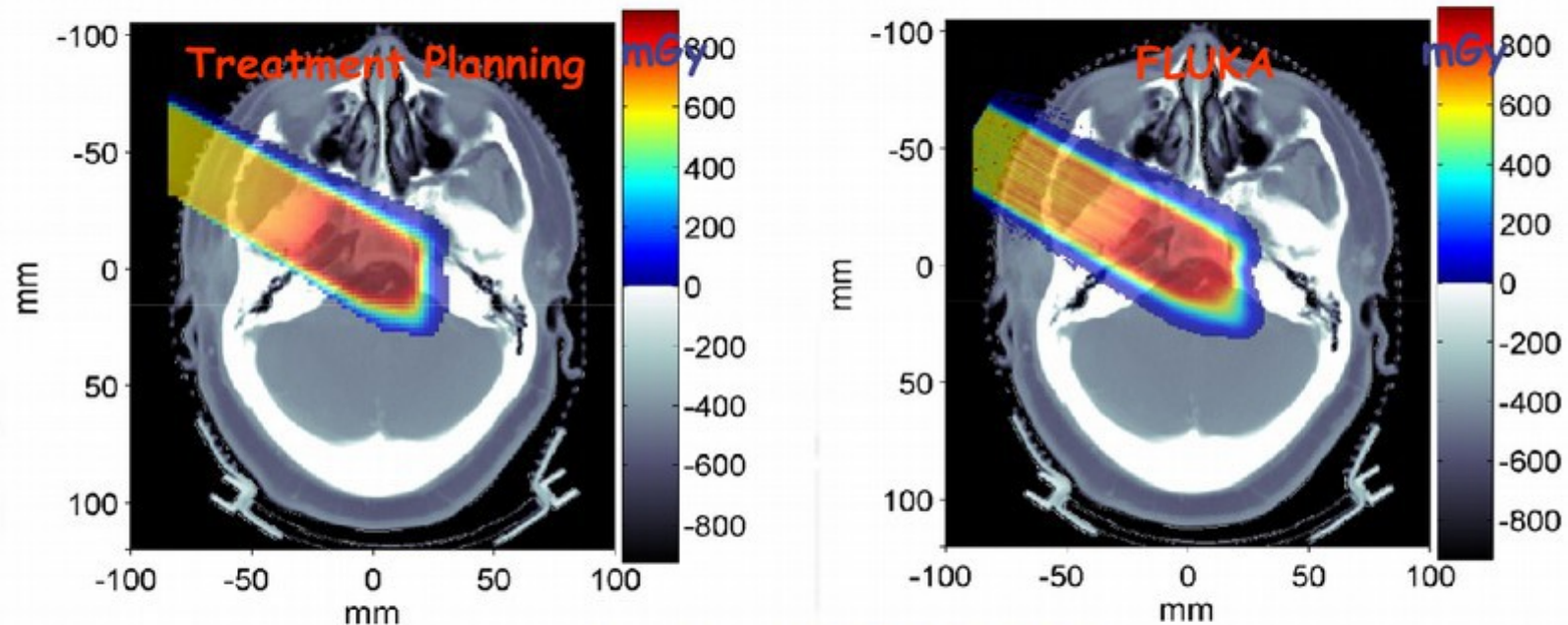
# Rationale for MC treatment planning

- AAPM report #85 (Papanikolaou et al 2004)
  - Due to steep slope of TCP and NTCP a 5% dose error can lead to a TCP change of 10-20% and worse for NTCP.
  - Prescribed → delivered dose, ~ 5% ( $1\sigma$ )
  - Improving dose engine, better than 3% ( $1\sigma$ )
- Tissue heterogeneities
  - Conventional superposition/convolution techniques give 5-10% deviations in heterogeneity (Mohan et al 1997) (e.g. lung), seen 15% for electrons (Ma et al 1999)



# MC – Tissue Heterogeneity

## Proton therapy: MC vs Focus/XiO for a Clivus Chordoma Patient at MGH



*Parodi et al, JPCS 74, 2007*

Prescribed dose: 1 GyE

MC :  $\sim 5.5 \cdot 10^6$  protons in 10 independent runs

(11h each on Linux Cluster mostly using 2.2GHz Athlon processors)

# *Dosimetry*

- Tools for determination of dose:

## • **Experimental**

- Ionisation chambers
- Solid state detectors
- Calorimetry
- Chemical dosimeters
- etc. etc

## • **Calculation tools**

- Paper and pencil (analytical)
- Exact numerical solution
- Pencil beam / collapsed cone
- Monte-Carlo codes

Calculation tools are also needed to establish necessary correction factors for dosimetry, e.g.:

- stopping power ratios,
- fluence correction factors,
- relative effectiveness

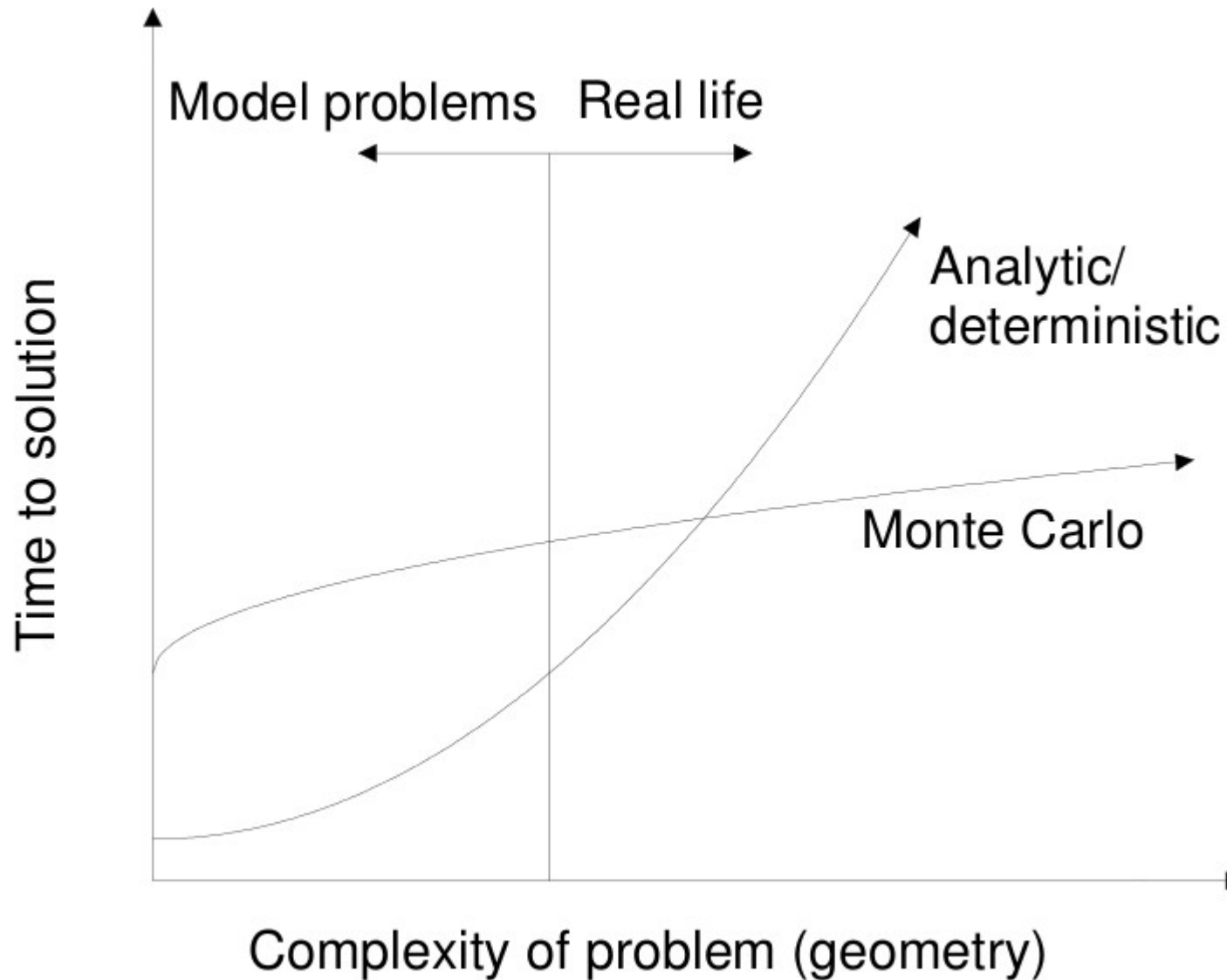
are **dependent** on the charged particle **fluence** spectrum

# Monte Carlo Algorithms

- Often pencil+paper or **analytical** calculations are impossible, e.g.:
  - when CPE does not apply
  - when geometries are complicated
  - dealing with fluence spectra
- **Numerical** calculations becomes quickly be impossible due to *many degrees of freedom* in complex geometries and multitude of physics models
- **Monte Carlo** (MC) techniques can help
  - Idea by E. Fermi and S. Ulam while they worked with shielding (?) at Los Alamos
  - MC particle transport: follow particle and interaction histories, when plenty, it simulates real life
  - == solving the radiation transport equation with MC methods!
  - Widespread use limited by **computing power**



## Monte Carlo *vs* deterministic/analytic methods



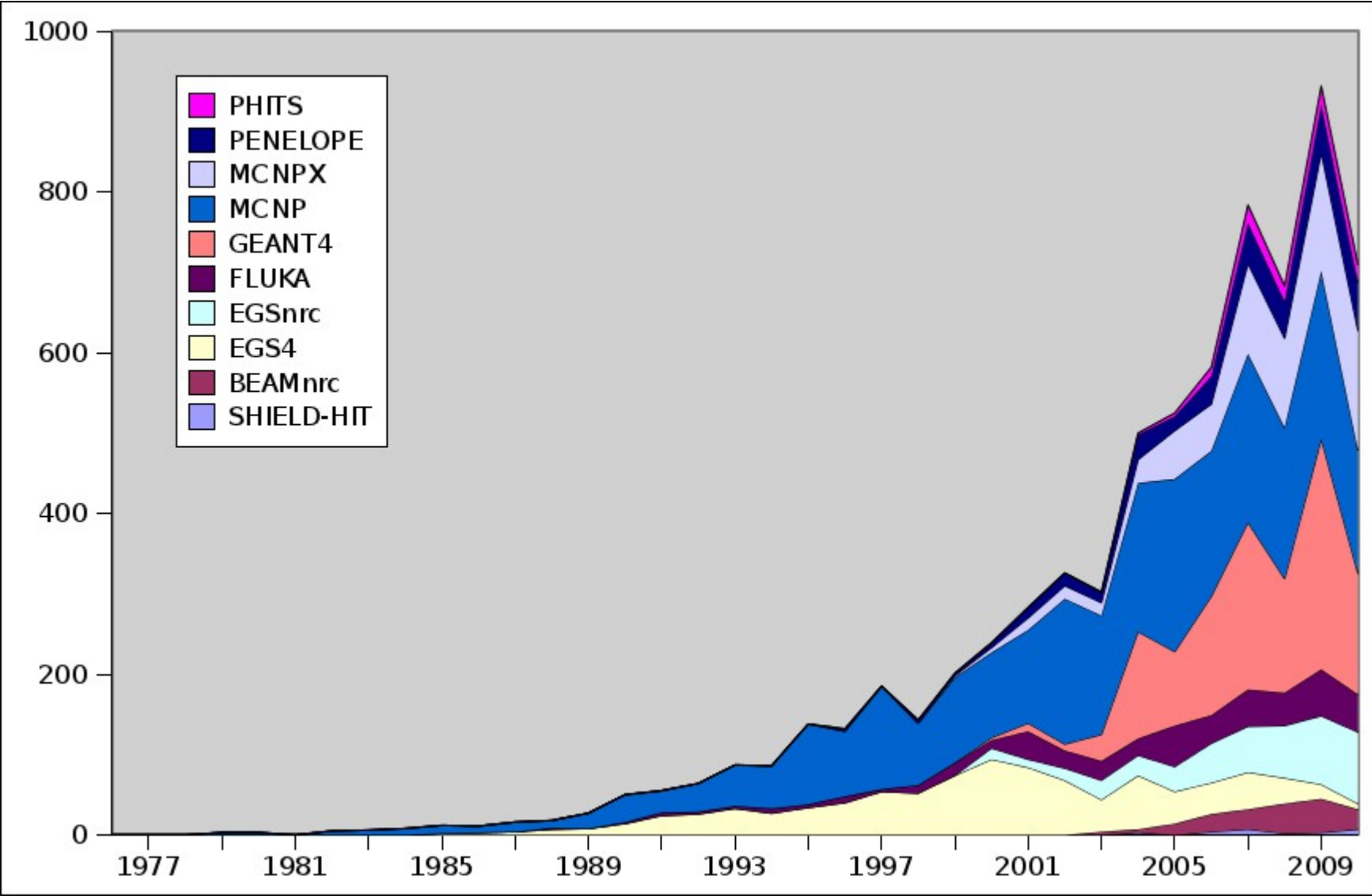
# Common MC Codes

- Photons & Electrons only
  - EGS4, EGSnrc, BEAMnrc (National Research Council of Canada)
  - Penelope (Facultat de Fisica (ECM), Universitat de Barcelona)
  - MCNP (including neutrons)
- Photons & Electrons + Ions
  - FLUKA (CERN)
  - Geant4 (CERN)
  - PHITS (Japan Atomic Energy Agency)
  - MCNPX (Los Alamos National Laboratory)
- Ions only:
  - SHIELD(-HIT) (Institute for Nuclear Research RAS)

# Common MC Codes in Use

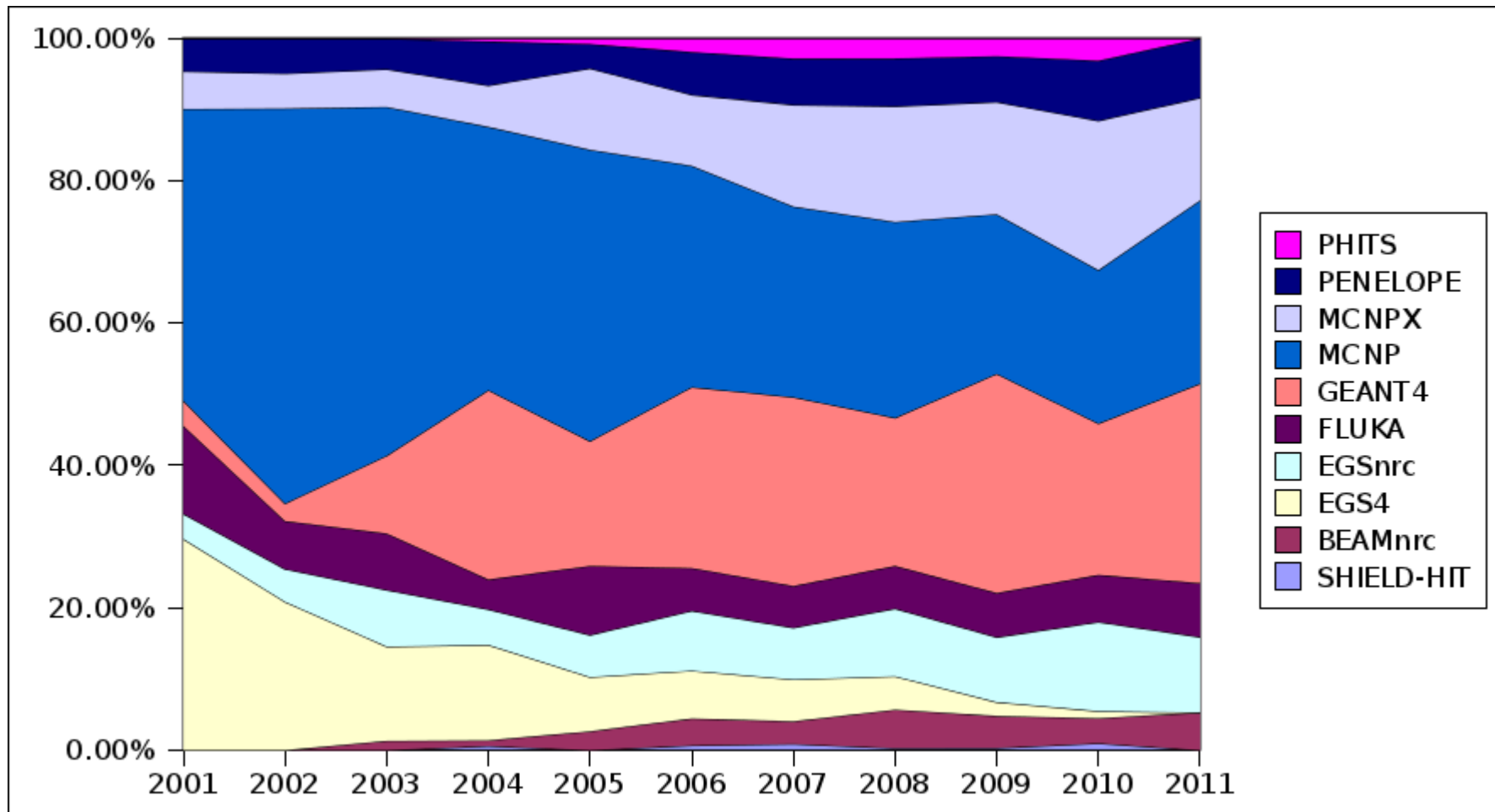
Number of publications

ISI Web of Knowledge



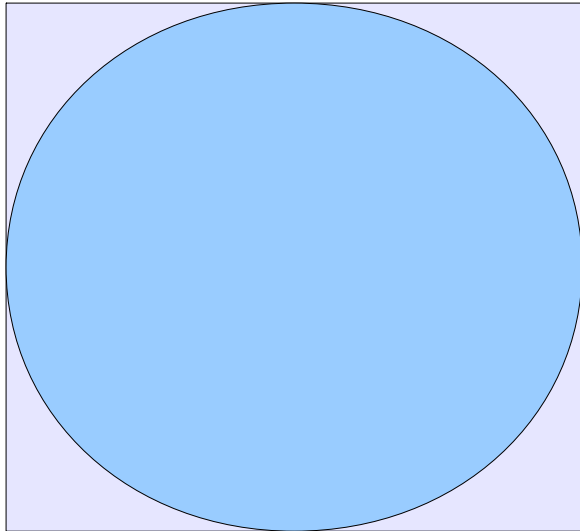
Year

# Common MC Codes in Use



# Monte Carlo Techniques

# Throwing Darts



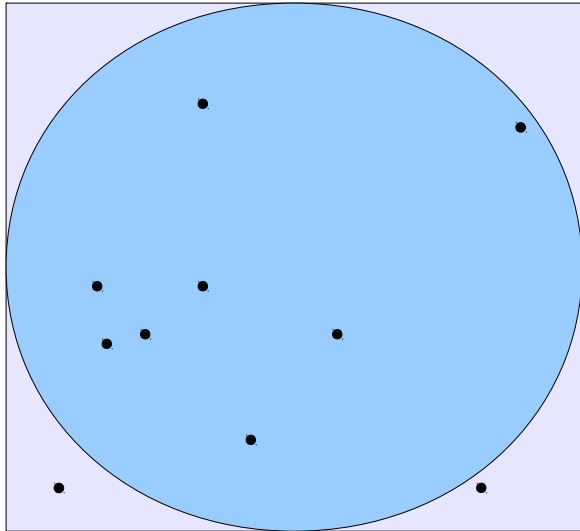
Area of square =  $(2r)^2$

Area of circle =  $\pi r^2$

Ratio of areas circle/square

=  $\pi/4 = 0.785398\dots$

# Throwing Darts



$$\text{Area of square} = (2r)^2$$

$$\text{Area of circle} = \pi r^2$$

$$\text{Ratio of areas circle/square}$$

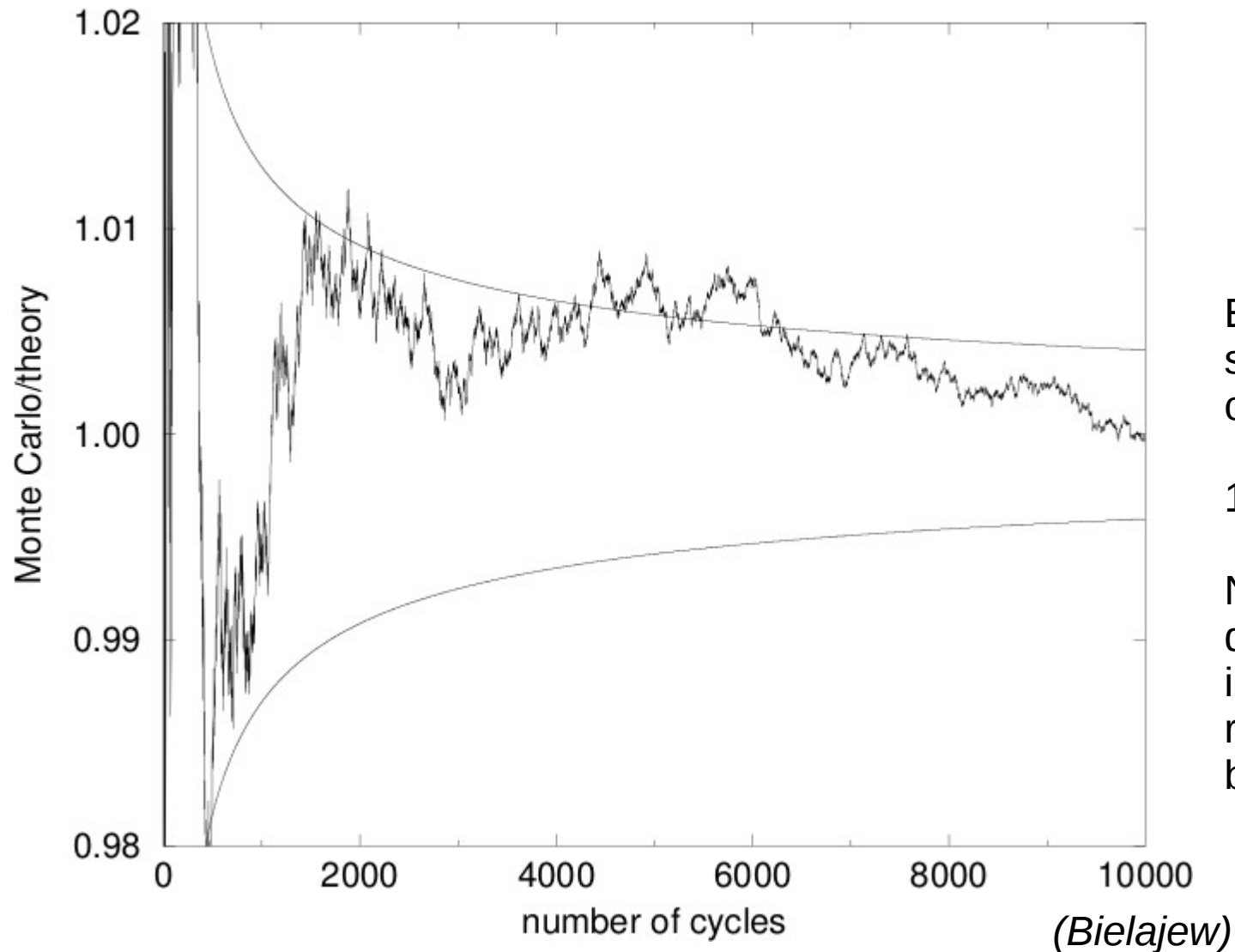
$$= \pi/4 = 0.785398\dots$$

Throwing  $N = 10$  darts

8 inside circle, 10 inside square  $\rightarrow 8/10 = 0.800\dots$

increase  $N$  for more precision

## Monte Carlo determination of $\pi$



Error has  
slow  
convergence:

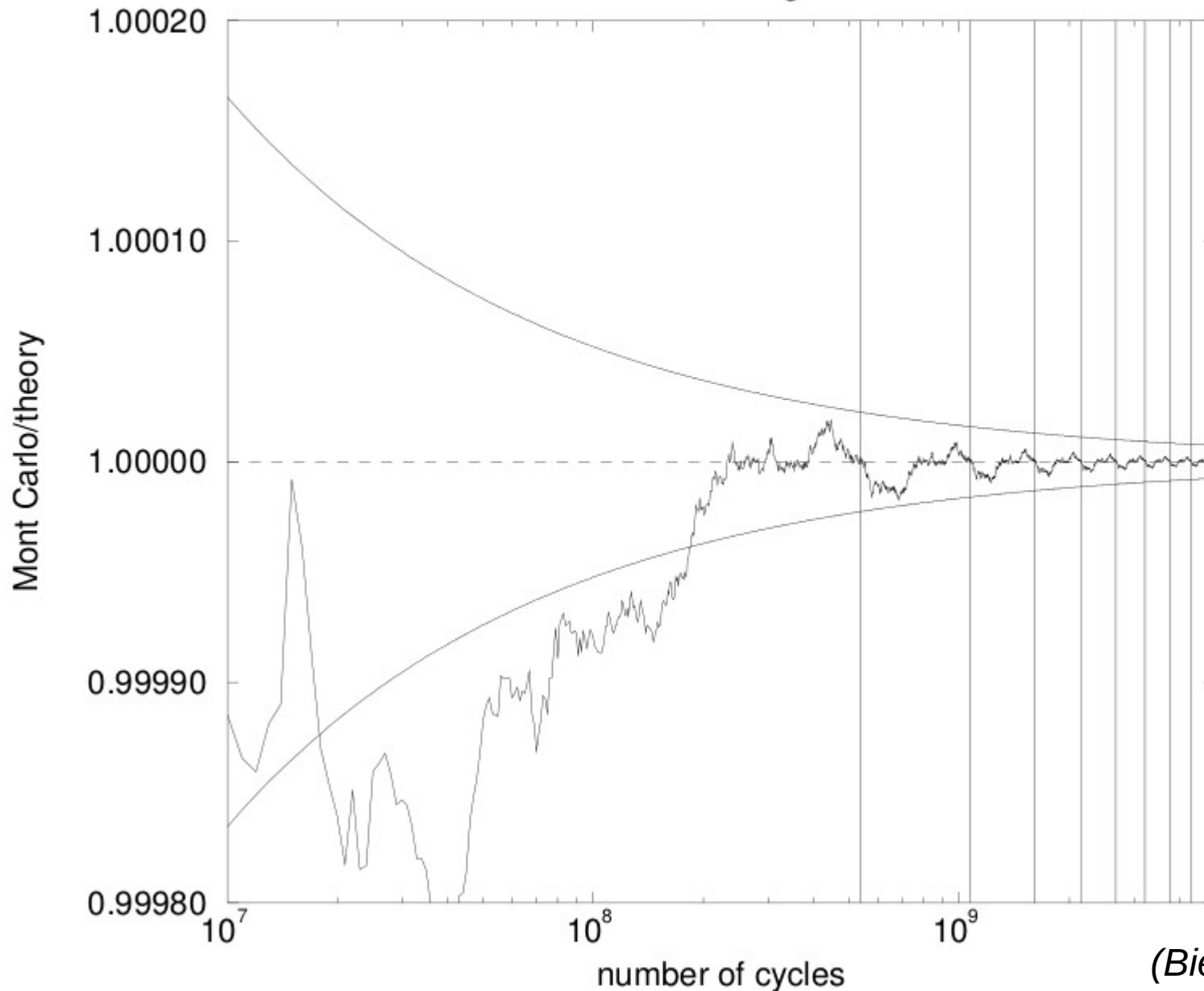
$1/\sqrt{N}$

Need to  
quadruply  $N$   
in order to  
reduce error  
by factor of 2.



# Determination of $\pi$

*trouble for large N*



*Example of false convergence due to insufficient random numbers.*

(Bielajew)

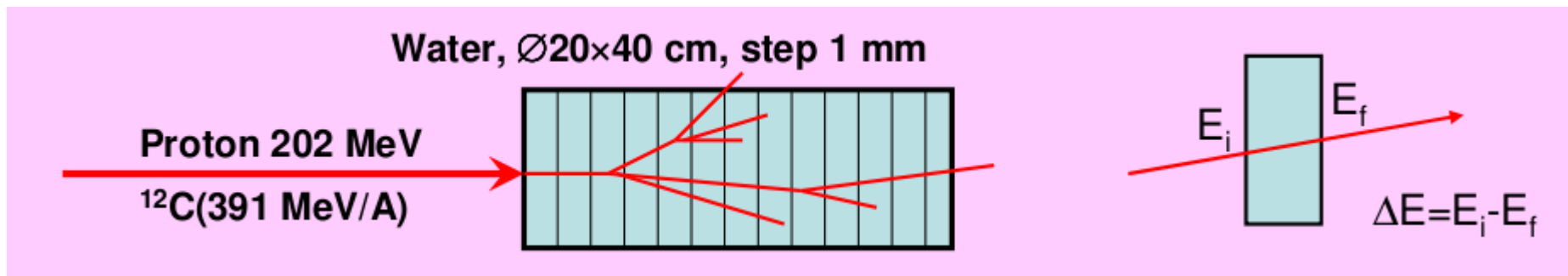
# Random numbers in MC algorithms

- Default random number generators (e.g. rand() of stdlib in c) are usually sh\*t and not applicable for serious MC calculations.
- Plenty of different random number generators exist
  - MCRNG, LCRNG, RANLUX, RANSHI ...
  - Sequence lengths of e.g.  $10^{19}$  random numbers
- Avoid experiments, use configurations and seeds which are well tested
- Several “random number” **hardness** testing packages exist (e.g. DIEHARD)
- Beware of **pitfalls** when parallelizing MC computations (e.g. accidentally running 100 parallel runs with same RND sequence)

# MC Particle Transportation

# MC Particle Transportation

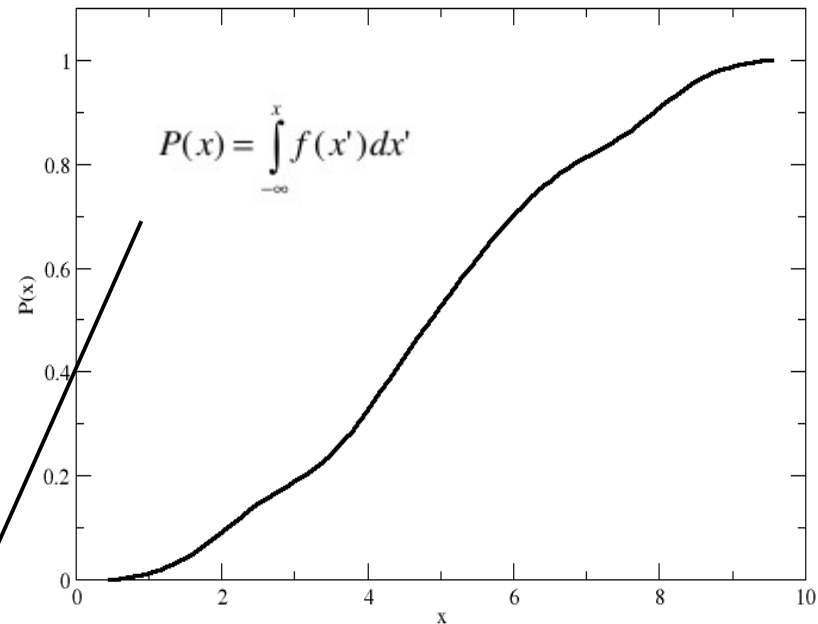
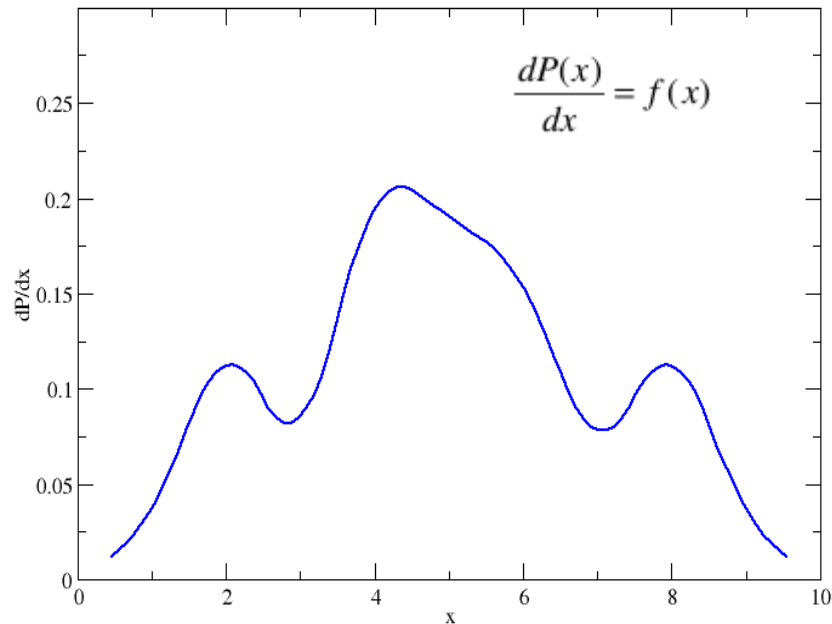
- MC particle transport:
  - Include probability distributions of all relevant physics
  - follow particle and interaction histories, when plenty, it simulates real life



- Conservation of **energy** and **momentum** are always obeyed.
- Relies on good random number generator

# Monte Carlo – Probability Distributions

$$1 = \int_{-\infty}^{\infty} f(x') dx'$$



Cumulative distribution function (CDF).  
The probability to measure  $P(x)$  is described by number between  $[0;1]$

$$r = P(x)$$

**The MC trick:** invert function, fill in a (flat distributed) random number  $r [0;1]$ , and get  $x$ .

$$x = P^{-1}(r)$$

Repeat a lot of times to get realistic simulation of  $f(x)$ .

# Example: Compton Scattering



The distance before next interaction,  $l$ , is a random variable.

We need to find its probability distribution, so we can convert a flat probability  $R$  [0:1] to the probability for next interaction.

cross section per atom :  $\sigma(E,z)$

nb of atoms per volume :  $n_{\text{at}} = \frac{\rho N}{A}$

cross section per volume :  $\eta(E, \rho) = n_{\text{at}} \sigma$  ( $\eta$  is in 1/cm )

- $\eta(E, \rho)$  is the probability of Compton interaction per cm
- $\lambda(E, \rho) = \eta^{-1}$  is the mean free path associated to the process (Compton)

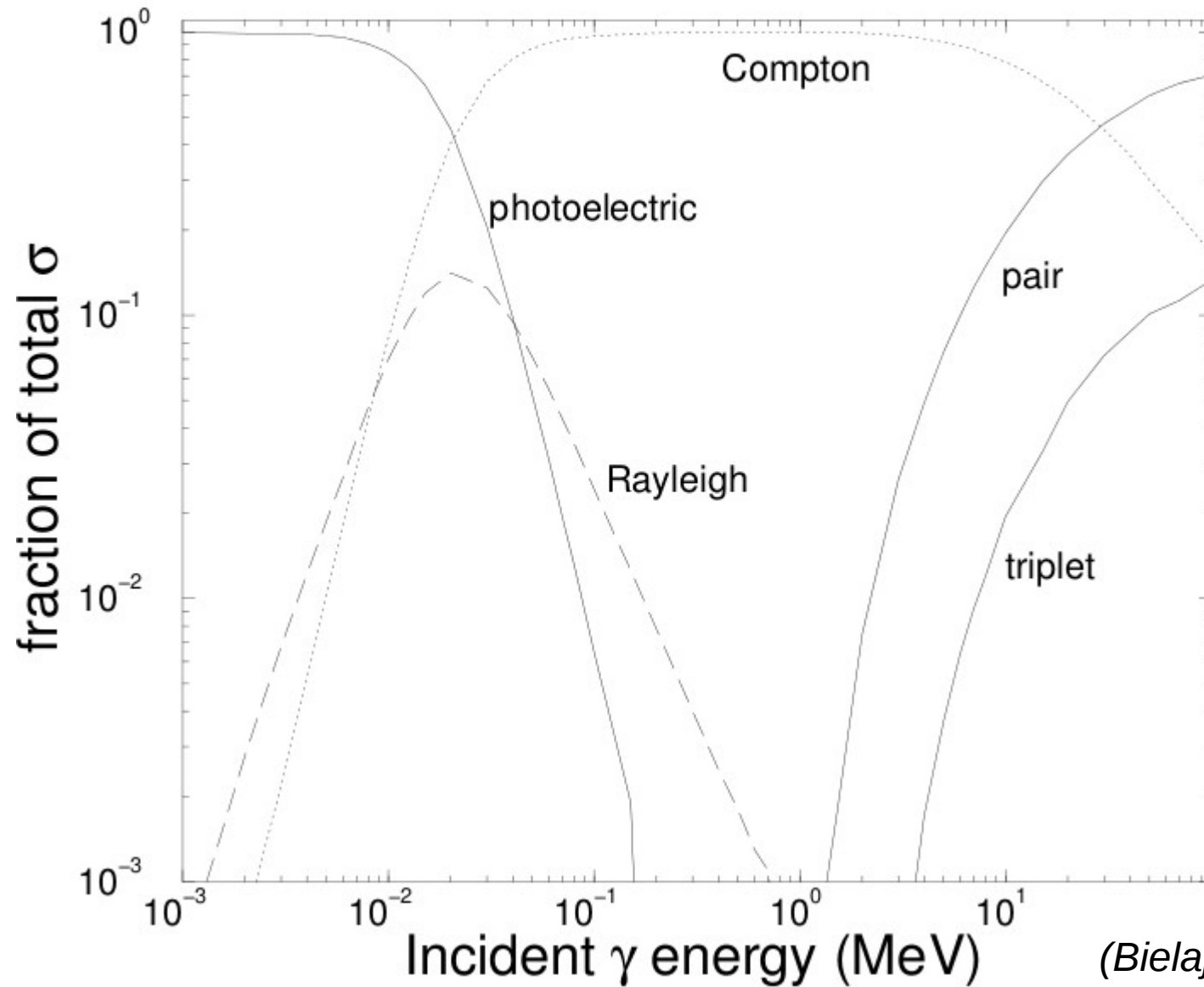
The probability distribution of  $l$ :  
Invert it, and substitute  $f(l)$  with  
random number  $R$ :

$$f(l) = \eta \exp(-\eta l) = \frac{1}{\lambda} \exp(-\lambda^{-1} l)$$
$$\ln(R \lambda) \lambda = l$$

Similar calculation can be done for angles of scattering, for the photon and electron.  
This is just one example, there is tons of physics implemented in similar ways

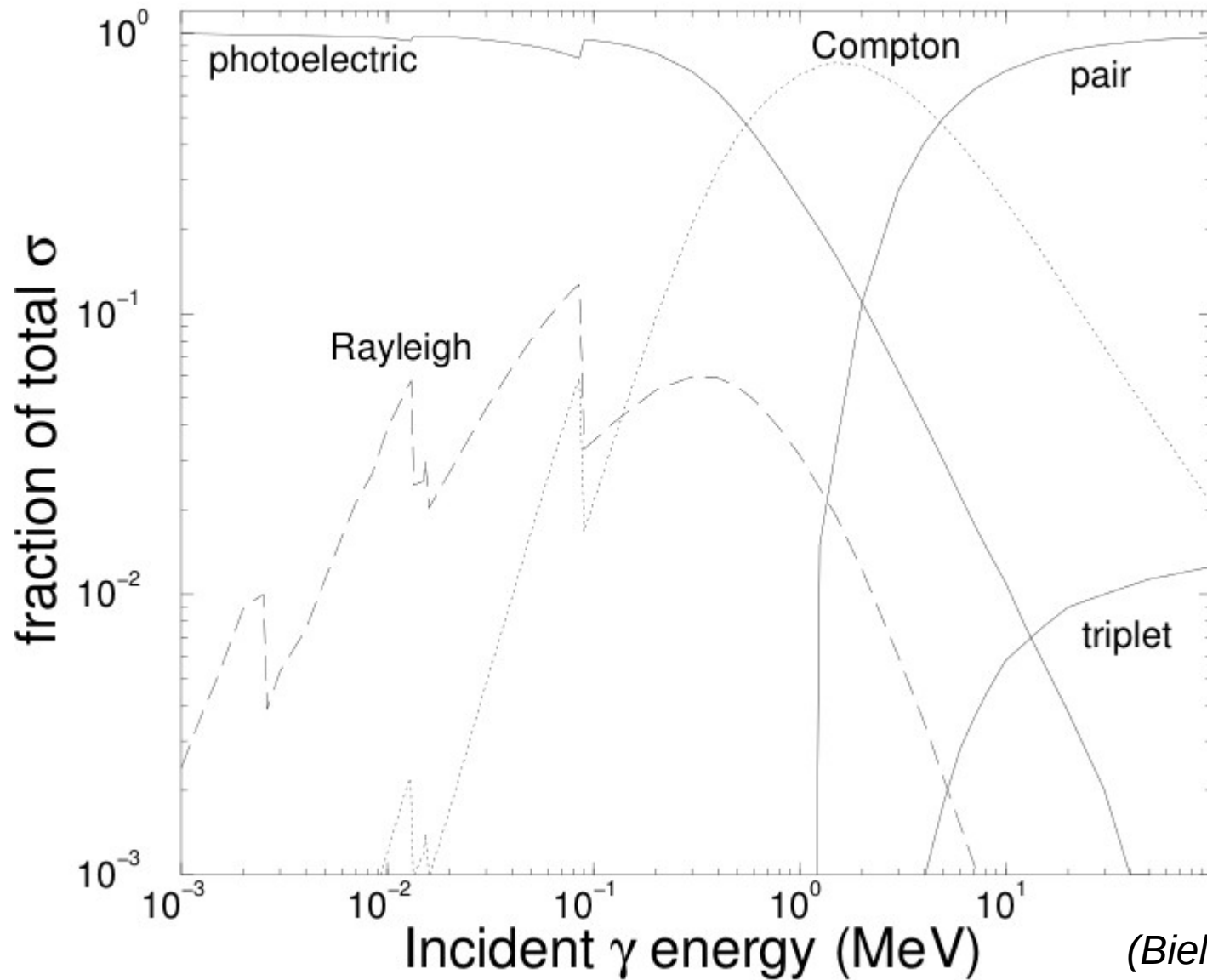
# Photon Interactions – Reaction Channels

Components of  $\sigma_\gamma$  in C



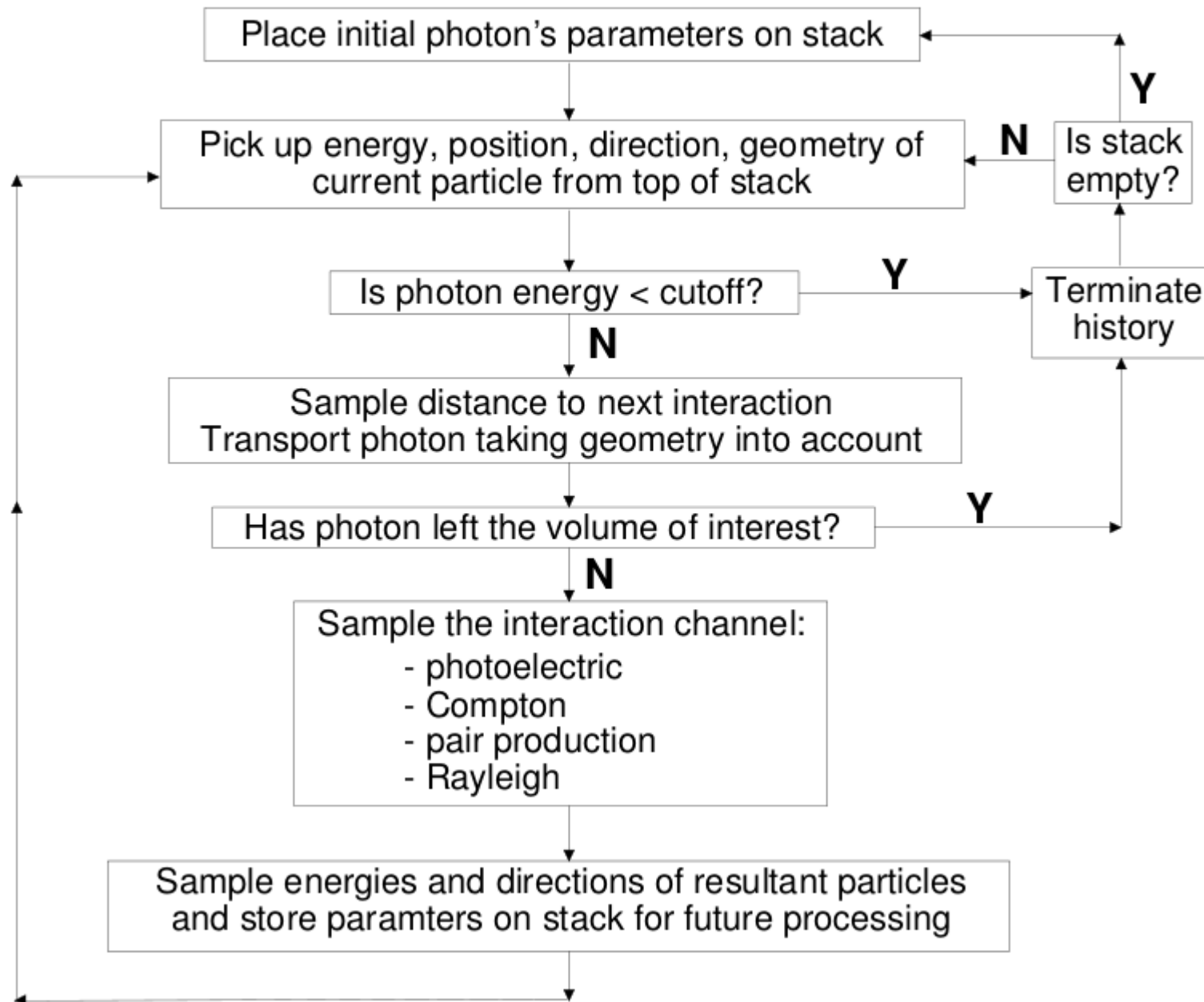
# Photon Interactions

## Components of $\sigma_\gamma$ in Pb





# Photon Transport



# Charged Particle Interactions

- A single 1 MeV ***photon***:
  - Number of interactions app. 10, i.e.  $\sim 10$  ions created by photon.
- A single 1 MeV ***charged particle***:
  - Large number of interactions,  $\sim 10^4$  ions created

Not feasible in MC (depending on the task to be solved),  
very CPU intensive for necessary precision.

Q: in what disciplines would you want a full *ab-initio* simulation?

# Groups of Charged Particle Interactions

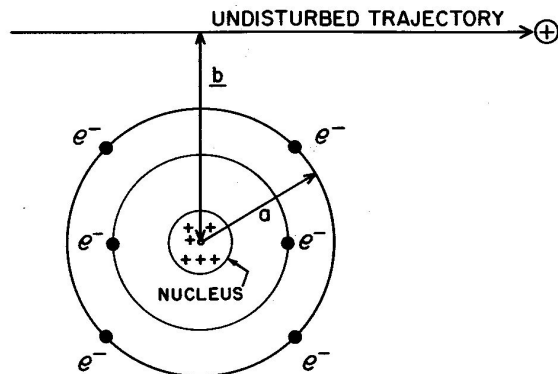


FIGURE 8.1. Important parameters in charged-particle collisions with atoms:  $a$  is the classical atomic radius;  $b$  is the classical impact parameter.

( $b \gg a$ ): **Soft collisions** Coulomb interaction with the whole atom. Large number of interactions. Small energy transfers.

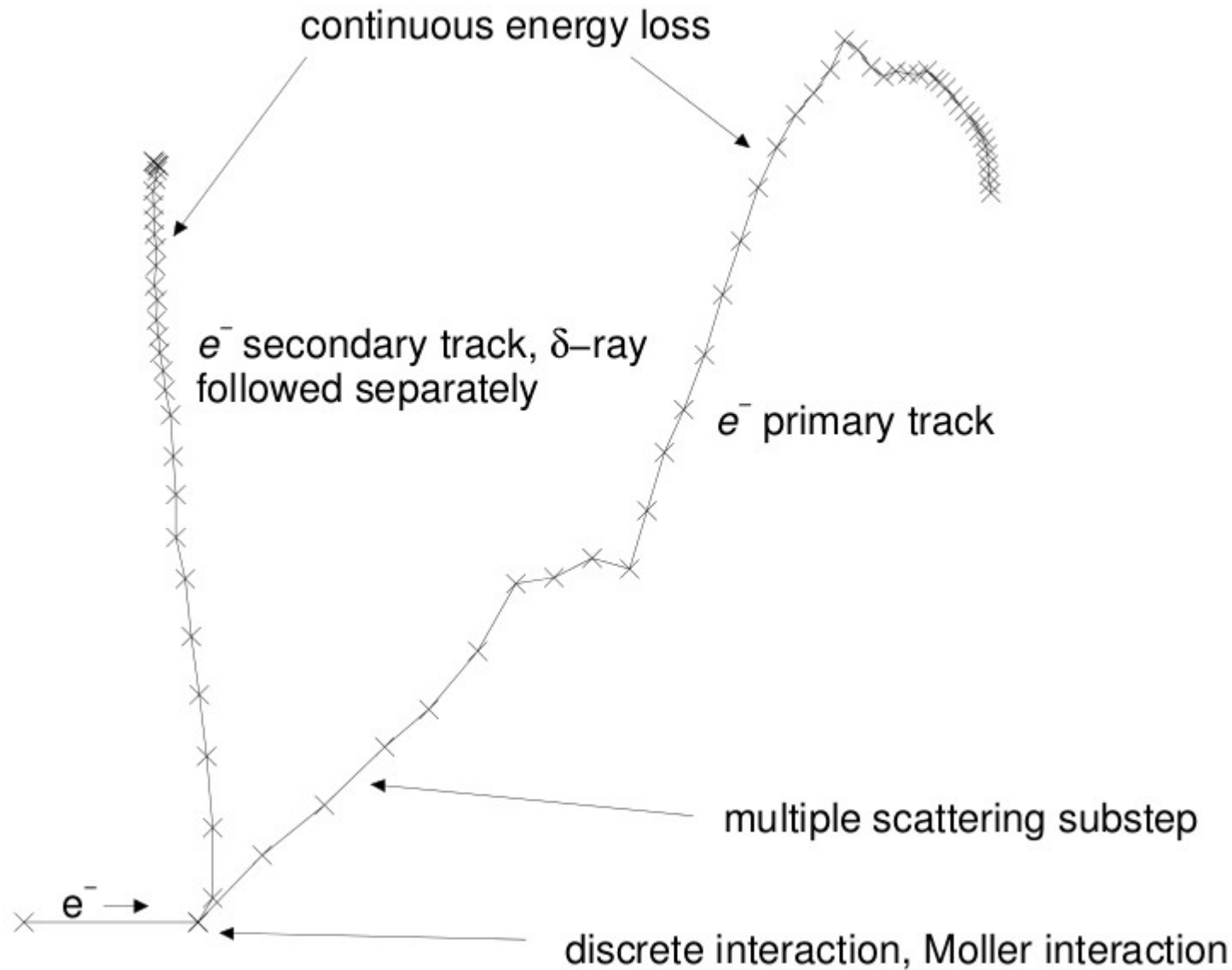
( $b \approx a$ ): **Hard collisions** Coulomb interaction with a single atomic electron. Large energy transfers. Creation of  $\delta$ -particles (high energy  $e^-$ )

( $b \ll a$ ): **Interactions with the nuclear field**

For incident electrons:  
Elastic scattering (resulting in multiple scattering).

Occasionally: Inelastic scattering. Creation of bremsstrahlung.

# Simulation of a single electron track



# Electron MC Transportation

- “Catastrophic”

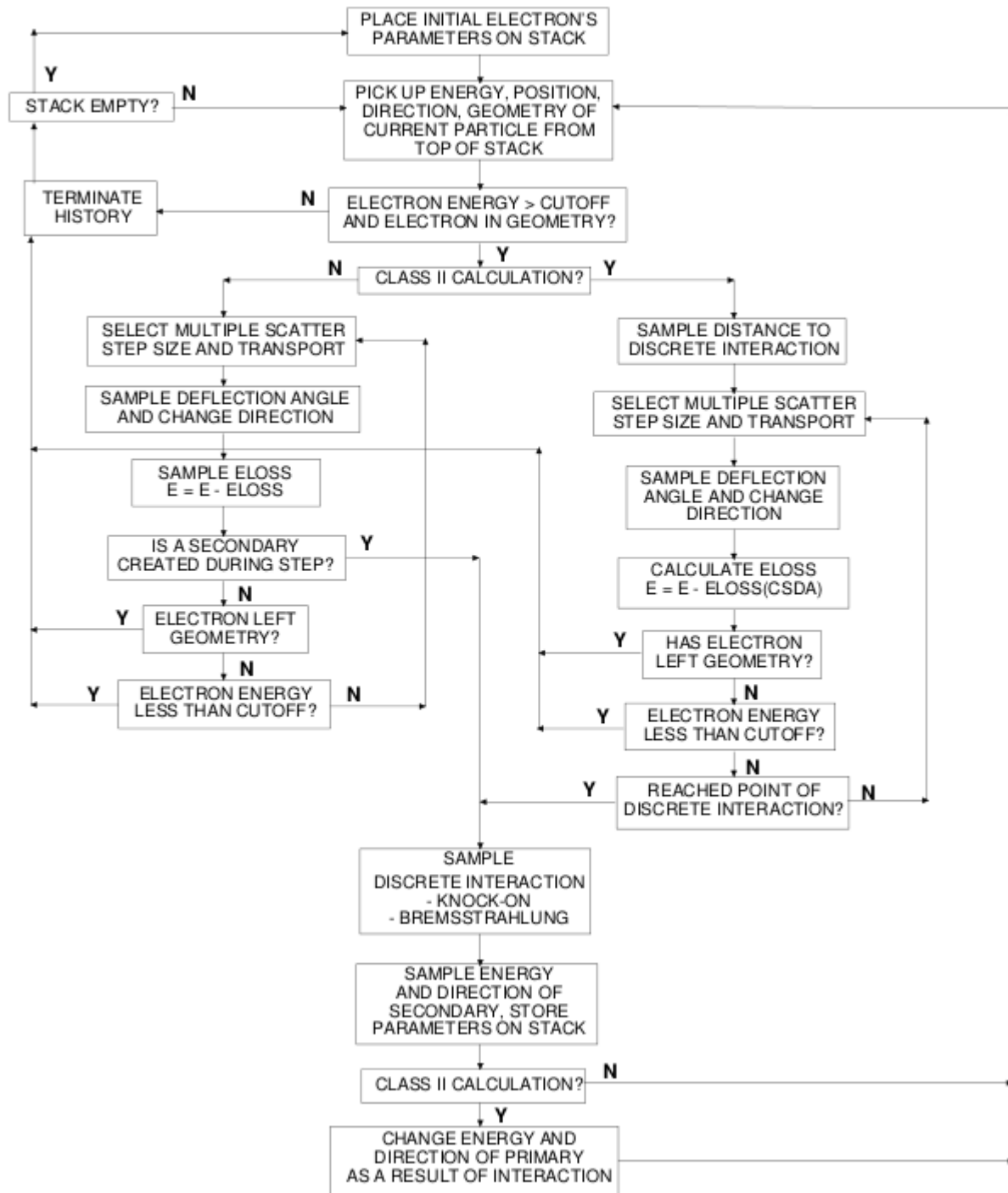
- large energy-loss Møller scattering ( $e^-e^- \longrightarrow e^-e^-$ ),
- large energy-loss Bhabha scattering ( $e^+e^- \longrightarrow e^+e^-$ ),
- hard bremsstrahlung emission ( $e^\pm N \longrightarrow e^\pm \gamma N$ ), and
- positron annihilation “in-flight” and at rest ( $e^+e^- \longrightarrow \gamma\gamma$ ).

- “Soft”

- low-energy Møller (Bhabha) scattering (modeled as part of the collision stopping power),
- atomic excitation ( $e^\pm N \longrightarrow e^\pm N^*$ ) (modeled as another part of the collision stopping power),
- soft bremsstrahlung (modeled as radiative stopping power), and
- elastic electron (positron) multiple scattering from atoms, ( $e^\pm N \longrightarrow e^\pm N$ ).

“Soft” interactions are small and numerous -> **condensed** simulation.

# Electron transport



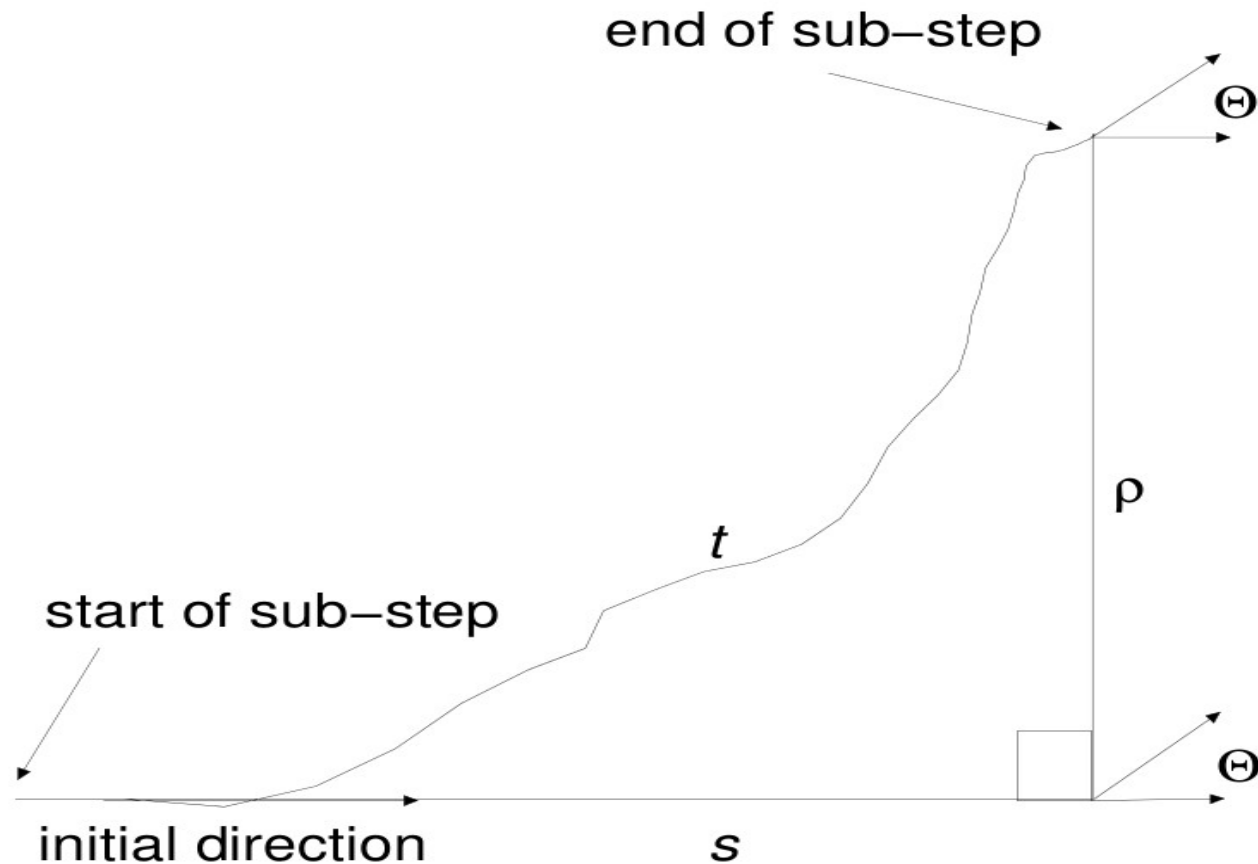
# Condensed MC

- charged particle interactions are not described individually (contrary to photon interactions)
- **Average effects** are described and put into groups

## *Examples of macroscopic (averaged) treatment of quantities in MC particle transport:*

- **Scattering** is described as “multiple scattering” (Moliere scattering, thin targets)
- **Stopping power  $dE/dx$**  is macroscopic
  - **Ions** are typically treated classically
  - **Electrons and positrons** are “always” relativistic
- **Energy fluctuations** “energy straggling” are described by Gaussian, Vavilov or Landau distributions.

# A single charged particle sub-step



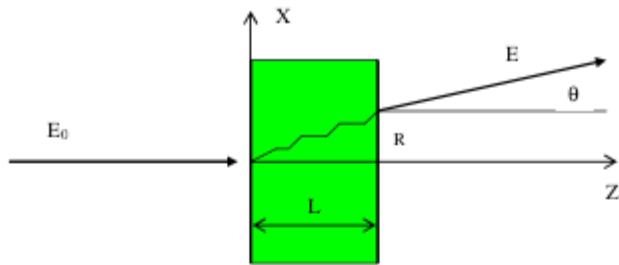
- **No simple relationship between  $t$  and  $s$**

- $\rho$  is often not calculated (ignored)

- Scattering is still happening due to  $\Theta$  (Moliere scattering)

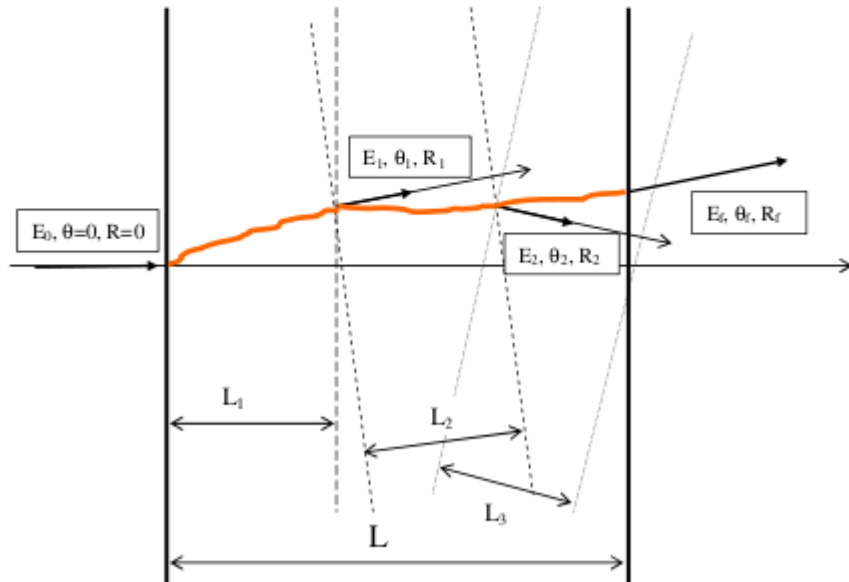
(Bielajew)





Прохождение тяжелой заряженной частицы с энергией  $E_0$  через слой вещества толщины  $L$ .

(Heavy ion transportation code SHIELD-HIT does take new position into account)



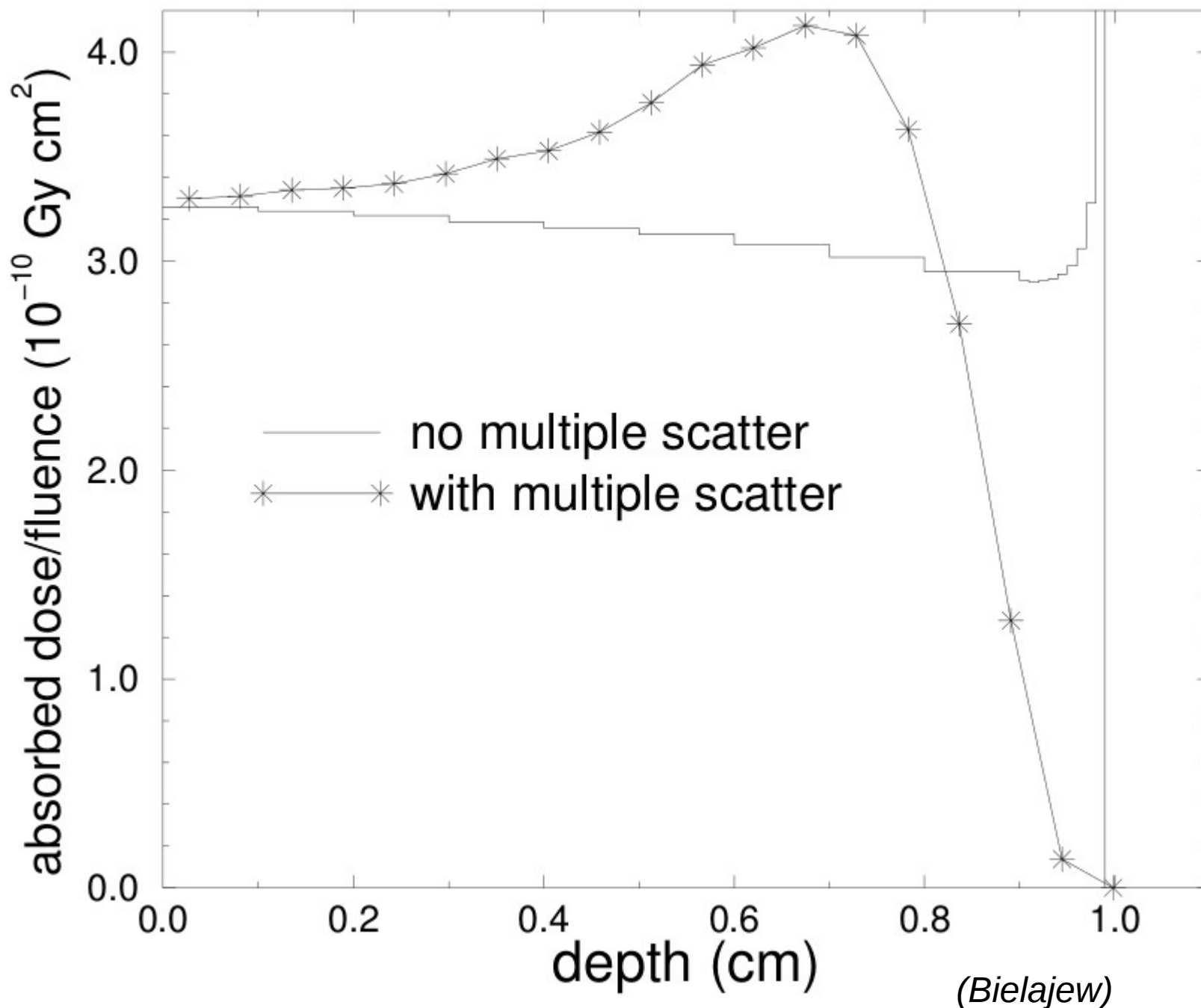
Слой толщины  $L$  как набор тонких слоев  $L_i$ .

$L$  is defined by user as a **minimum step length**, within this condensed physics is applied instead of discrete sampling

Typical ion step lengths: 5% energy loss (HADRONthe default FLUKA and SH12A)..

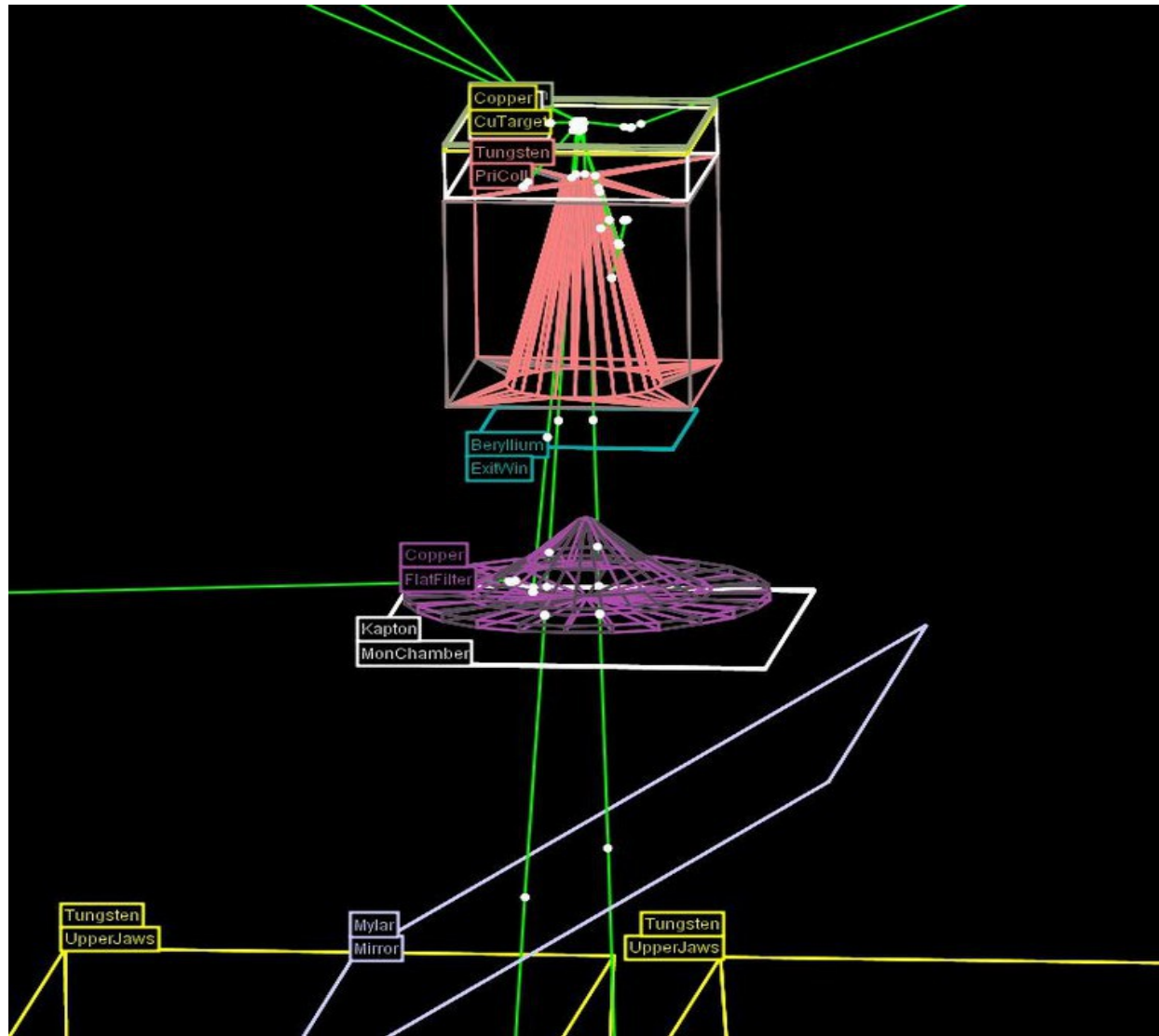
# 20 MeV $e^-$ on water

broad parallel beam, CSDA calculation



(Bielajew)

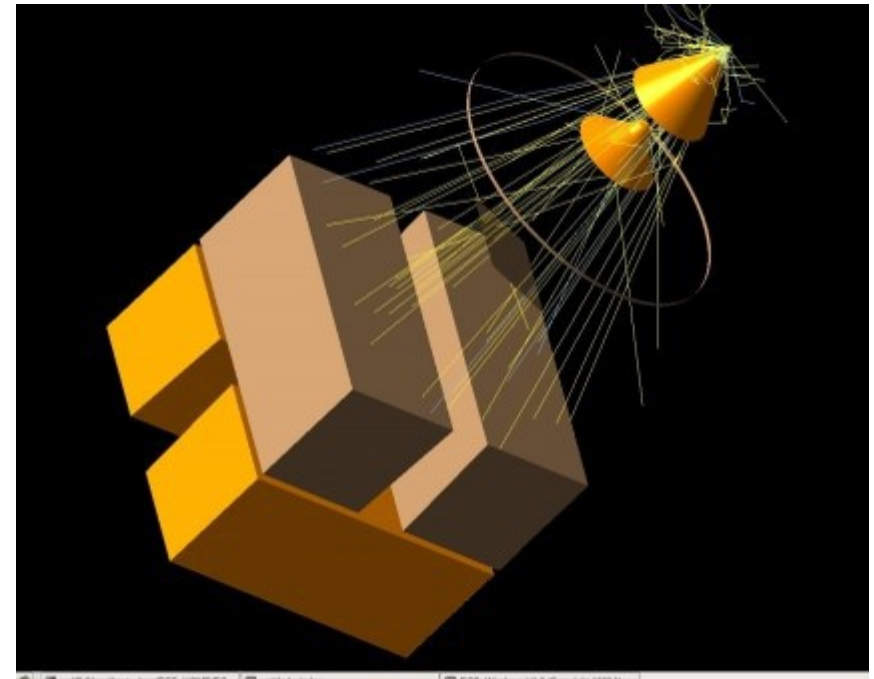
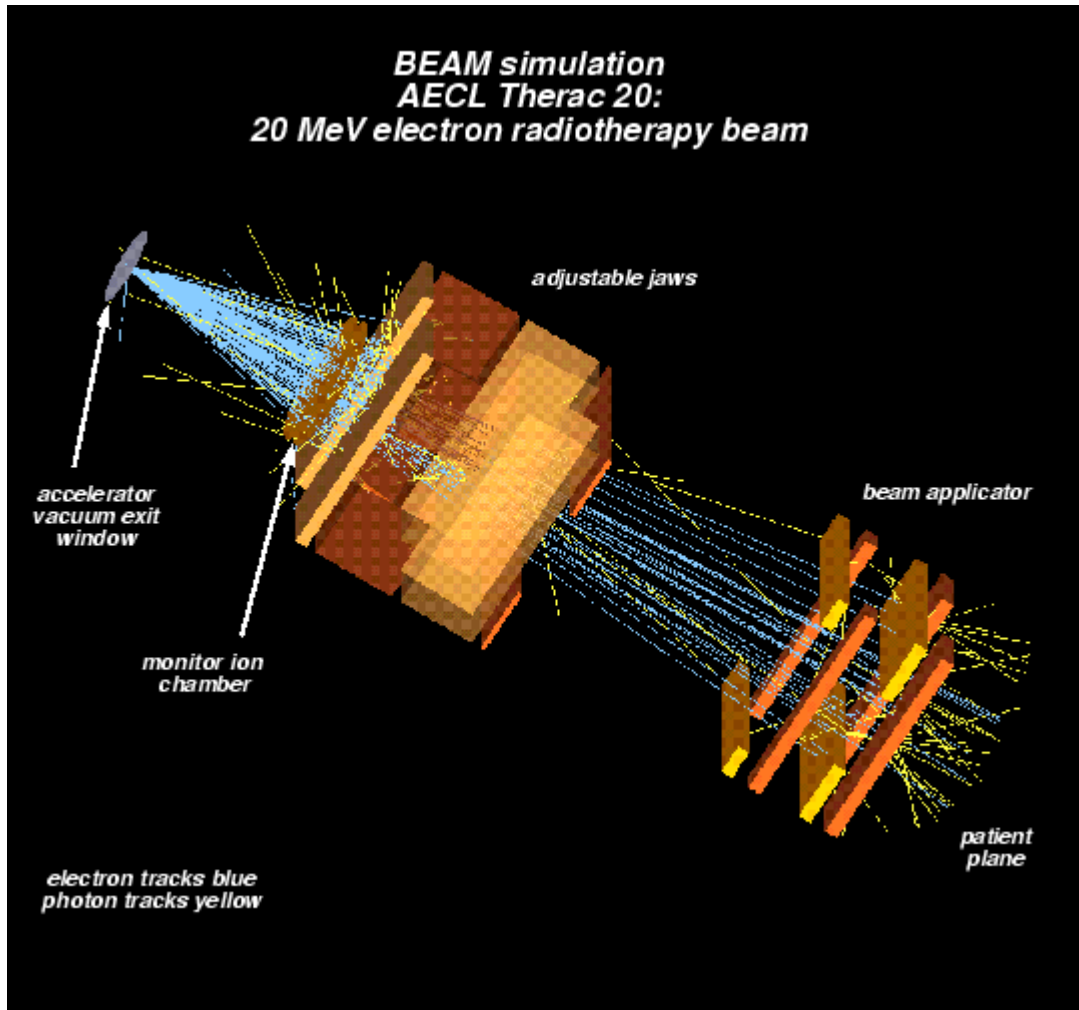
# Geometry Considerations



# Beam Sources

- 1) Full simulation of treatment head
- 2) Virtual treatment head
- 3) Phase space file of pre-calculated values

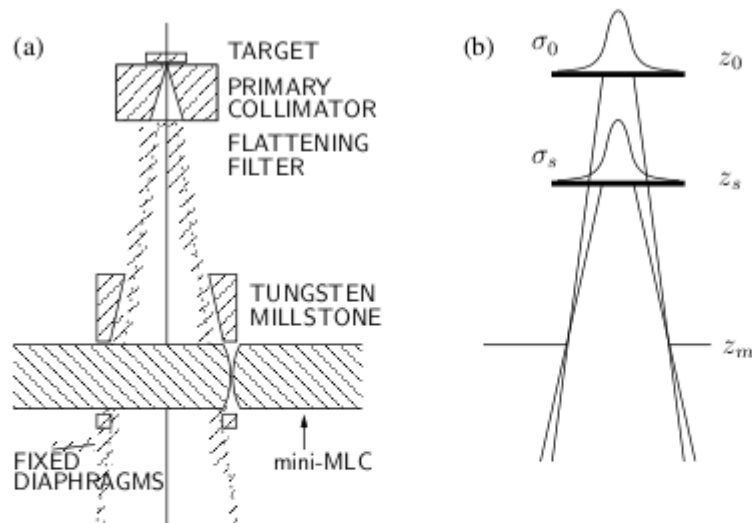
# 1) Full simulation



Photon therapy w. flattening filters

Electron beam application (BEAMnrc)

## 2) Virtual Source



**Figure 1.** (a) The collimation system of the EBM with marked positions of a target and a flattening filter. (b) Scheme of the VEF of the EBM, where  $\sigma_0$  and  $\sigma_s$  are standard deviations of the Gaussian intensity distribution of the primary and secondary photon sources respectively,  $z_0$  the position of the primary photon source,  $z_s$  the position of the secondary photon source and the electron contamination source,  $z_m$  the position of the upper edge of the mini MLC.

A Virtual Source Model (VSM) described the beam above the MLC.

(Sikora et al, PMB 2007)

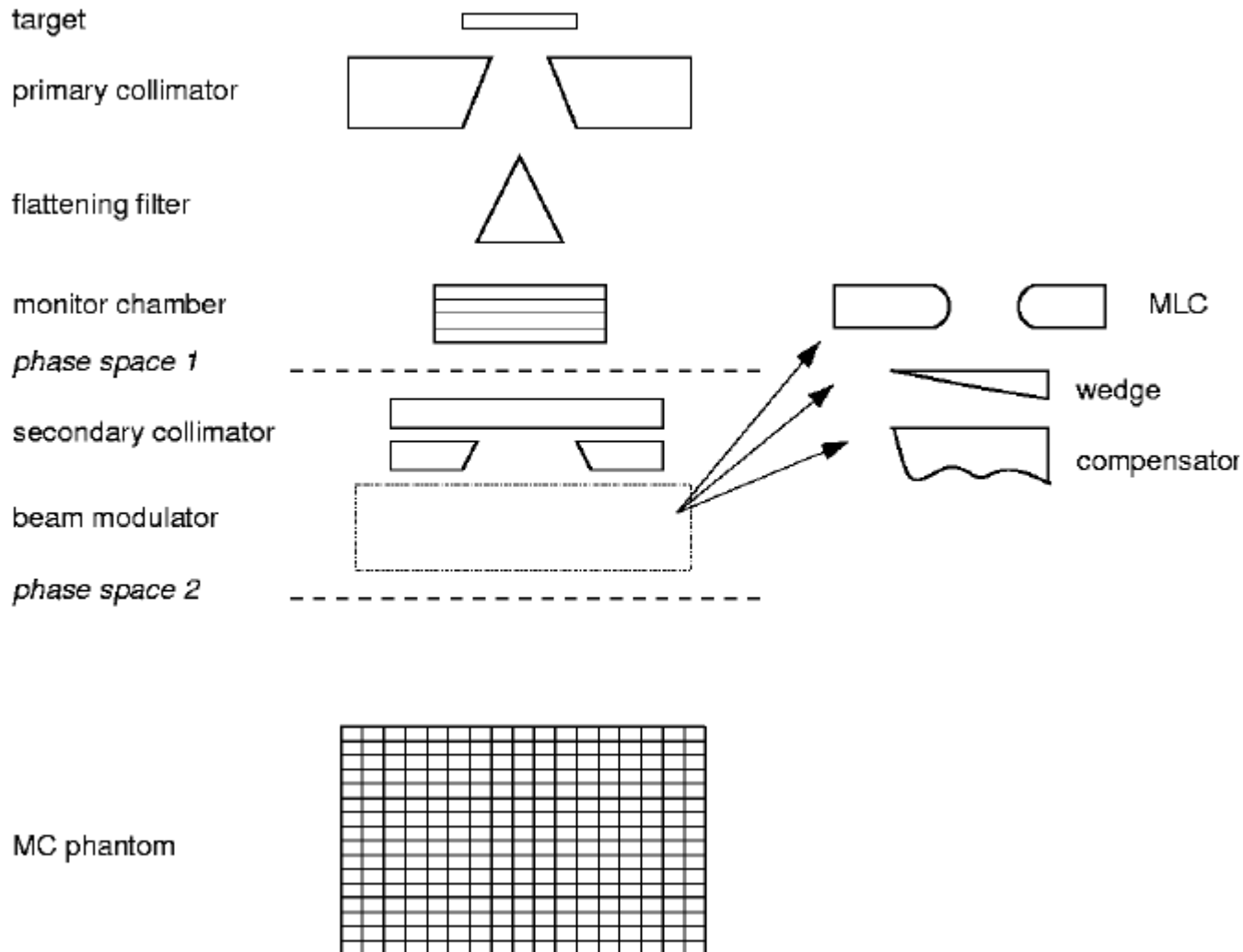
### 3) Using Phase Space Files

- Phase space file: list of particles, direction vector and energy
  - $n(x,y,z,v1,v2,E)$
- IAEA .phsp definition: <http://www-nds.iaea.org/phsp/phsp.htmlx>

IAEA provide a database with linacs and Co-60 phase-space files

Variable	Meaning	Type of variable
<b>X</b>	First coordinate (usually X position in cm)	Real*4
<b>Y</b>	Second coordinate (usually Y position in cm)	Real*4
<b>Z</b>	Third coordinate (usually Z position in cm)	Real*4
<b>U</b>	First direction cosine	Real*4
<b>V</b>	Second direction cosine	Real*4
<b>E</b>	Kinetic energy in MeV	Real*4
<b>Statistical_Weight</b>	Particle statistical weight	Real*4
<b>Particle_type</b>	Type of the particle <i>Current list:</i> photons, electrons, positrons, protons and neutrons	Integer*2
<b>Sign_of_W</b>	Sign of W (Third direction cosine)	Logical*1
<b>Is_new_history</b>	Signifies if particle belongs to new history	Logical*1
<b>Integer_extra</b>	Extra storage space for integer variables <i>Currently defined variables:</i> Incremental history number EGS LATCH PENELOPE ILB	$n*(Integer*4)$ ( $n \geq 0$ )
<b>Float_extra</b>	Extra storage space for real variables <i>Currently defined variables</i> XLAST YLAST ZLAST	$m*(Real*4)$ ( $m \geq 0$ )

### 3) Using Phase Space Files (cont.)



a representative recording of particles in a plane, typically (but not necessarily) before any modifies which are specific to the treatment.





# SMCP-Interface with Eclipse

External Beam Planning  
LUNG\_1  
Series\_1  
2-PLAN 2  
VMC  
VMC - Unapproved - Transversal  
VMC - Unapproved - Frontal

SMCP Gui  
File Options About  
General Config Research EPID

**Source Setting**

Select source

- Phase space file
- Source model
- Source model inc. jaws
- AAA source model
- VMC++
- VMC++ inc. jaws
- Use prepatient phsp

Jaw transport

- Transmission
- Jaw transport model

**Beam Modifier**

Jaw  
Geometry Exact Transport EGSnrc

Enhanced dynamic wedge  
Geometry Exact Transport EGSnrc

MLC  
Geometry Exact Transport EGSnrc

Upper wedge  
Geometry Exact Transport EGSnrc

Block  
Geometry Exact Transport EGSnrc

Lower wedge  
Geometry Exact Transport EGSnrc

**Dose Engine**

Select computation  
EGSnrc  
CT conversion EGSnrc

- Compute prepatient phsp
- Compute dose
- Load only dose file

Select Voxelsize

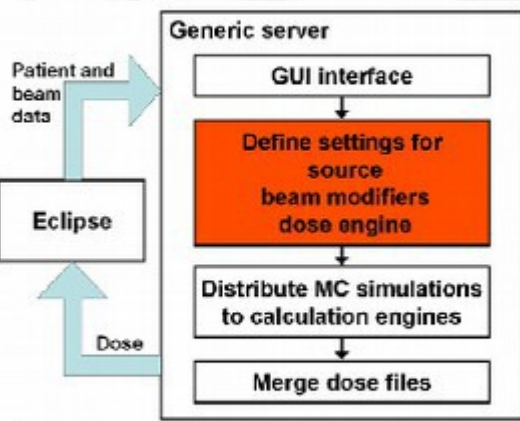
Voxelsize X 0.4  
Voxelsize Y 0.4  
Voxelsize Z 0.4

Variance reduction

- Particle splitting (100)
- Russian roulette
- Smooth dose

Execute Cancel

SMCP V0.5



# Calculation Speed

TABLE I. Summary of timing and accuracy results from the ICCR benchmark. Timing comparisons were performed using 6 MV photons,  $10 \times 10$  cm<sup>2</sup> field size, and those for the accuracy test, using 18 MV photons and a  $1.5 \times 1.5$  cm<sup>2</sup> field size, as detailed in the ICCR benchmark (Ref. 99). All times have been scaled to the time it would take running on a single, Pentium IV, 3 GHz processor. Readers should be aware that the timing results, as well as the method used to scale the times, are subject to large uncertainties due to differences in compilers, memory size, cache size, etc.

Monte Carlo code	Time estimate (min)	% mean difference relative to ESG4/PRESTA/DOSXYZ
ESG4/PRESTA/DOSXYZ	43	0, benchmark calculation
VMC++	0.9	$\pm 1$
XVMC	1.1 <sup>a</sup>	$\pm 1$
MCDOSE (modified ESG4/PRESTA)	1.6	$\pm 1$
MCV (modified ESG4/PRESTA)	22	$\pm 1$
DPM (modified DPM)	7.3 <sup>b</sup>	$\pm 1$
MCNPX	60 <sup>c</sup>	Maximum difference of 8% at Al/lung interface (on average $\pm 1$ % agreement)
PEREGRINE	43 <sup>d</sup>	$\pm 1$
GEANT4 (4.6.1)	193 <sup>e</sup>	$\pm 1$ for homogeneous water and water/air interfaces

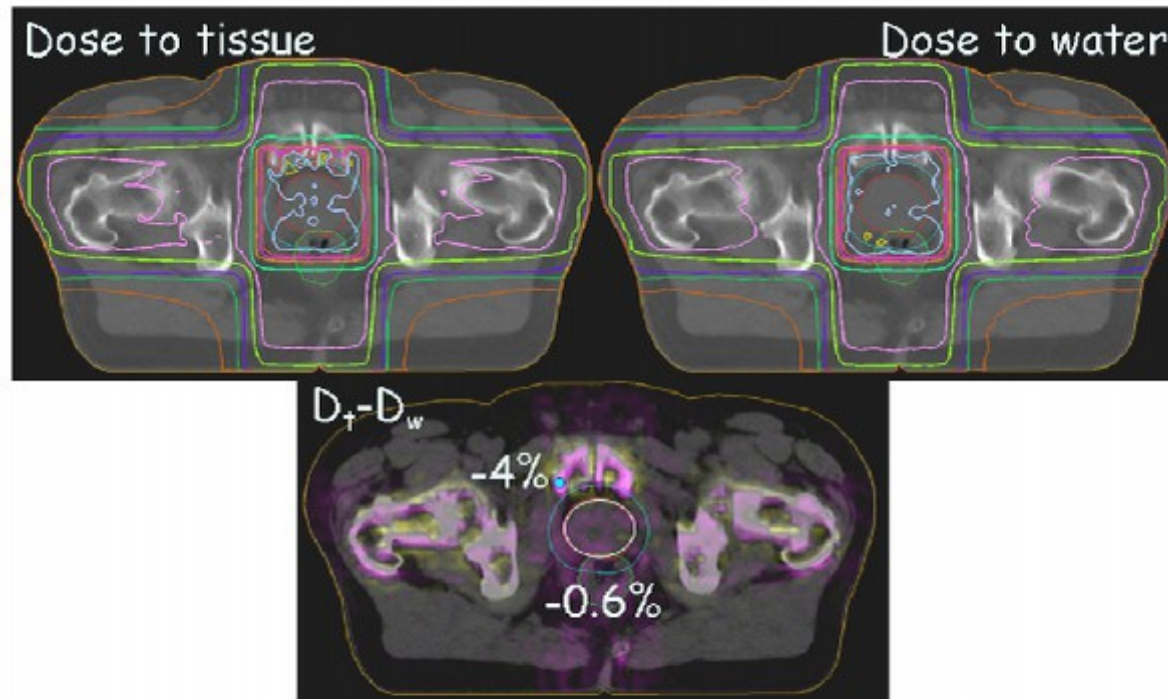
# Computer Clusters

← cluster  
maintained by  
APTG in  
Heidelberg



Future is cloud computing! See e.g. Amazon Web Services.

# Dose to Water vs Dose to Medium



**Figure 3.** The four-field box technique for the prostate case with MC calculations for all tissues mapped as tissues (upper left) and mapped as water (upper right). The difference is shown in the lower panel. The isodoses shown are 115, 112.5, 110, 107.5, 105, 102.5, 100, 97.5, 95, 90, 70, 50, 30, 10, 5 and 2%. The dose in cortical bone at the blue dot is  $-4\%$  and the average dose in the PTV is  $-0.6\%$  compared to the dose to water plan.

(Knöös et al, 2006, PMB)

# Dose to Water vs Dose to Medium

IOP PUBLISHING

PHYSICS IN MEDICINE AND BIOLOGY

Phys. Med. Biol. **56** (2011) 3073–3089

doi:[10.1088/0031-9155/56/10/012](https://doi.org/10.1088/0031-9155/56/10/012)

## **Dose specification for radiation therapy: dose to water or dose to medium?**

**C-M Ma<sup>1</sup> and Jinsheng Li**

Radiation Oncology Department Fox Chase Cancer Center, Philadelphia, PA 19111, USA

E-mail: [charlie.ma@fccc.edu](mailto:charlie.ma@fccc.edu)

Received 30 December 2010, in final form 27 March 2011

Published 20 April 2011

Online at [stacks.iop.org/PMB/56/3073](https://stacks.iop.org/PMB/56/3073)

MC codes calculated Dose to Medium. Should they be translated to dose to water?

# Dose to Water vs Dose to Medium

- (1) Conventional photon dose calculation algorithms, either correction based or model based, compute doses using water with different electron densities, which are close (<4% differences) to doses to media, as computed by Monte Carlo, but significantly different (up to 11%) from doses to water converted from doses to media following AAPM TG105 recommendations.
- (2) Our results suggest that for consistency with previous radiation therapy experience, Monte Carlo photon algorithms report dose to medium for radiotherapy dose prescription, treatment plan evaluation and treatment outcome analysis.

*(... except.)  
They also comment for electron plans:  
use water with varying electron density.*

(Ma et al. 2011 PMB)

# Monte Carlo – Usage Examples

- CMS and ATLAS detector at CERN
- Shielding in space, airplanes, accelerator vaults
- Nuclear fission and fusion reactors, -bombs
- ...

(FLUKA, Geant4)

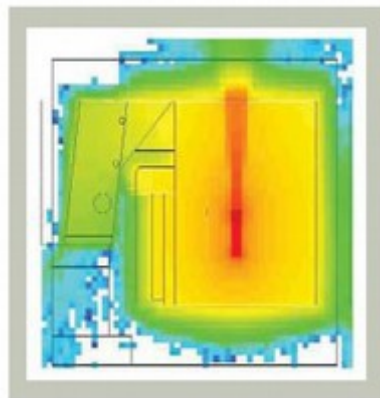
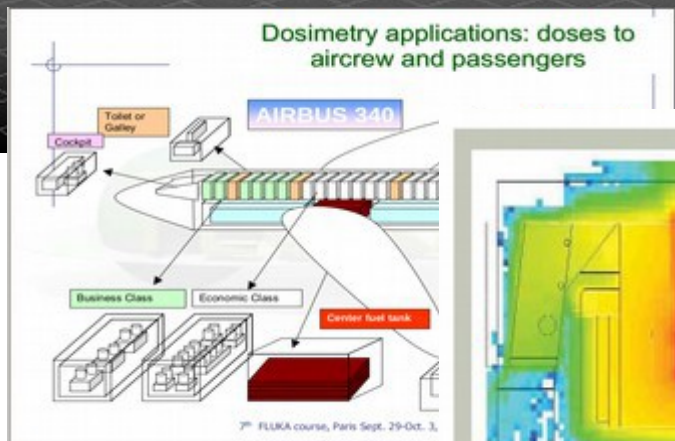
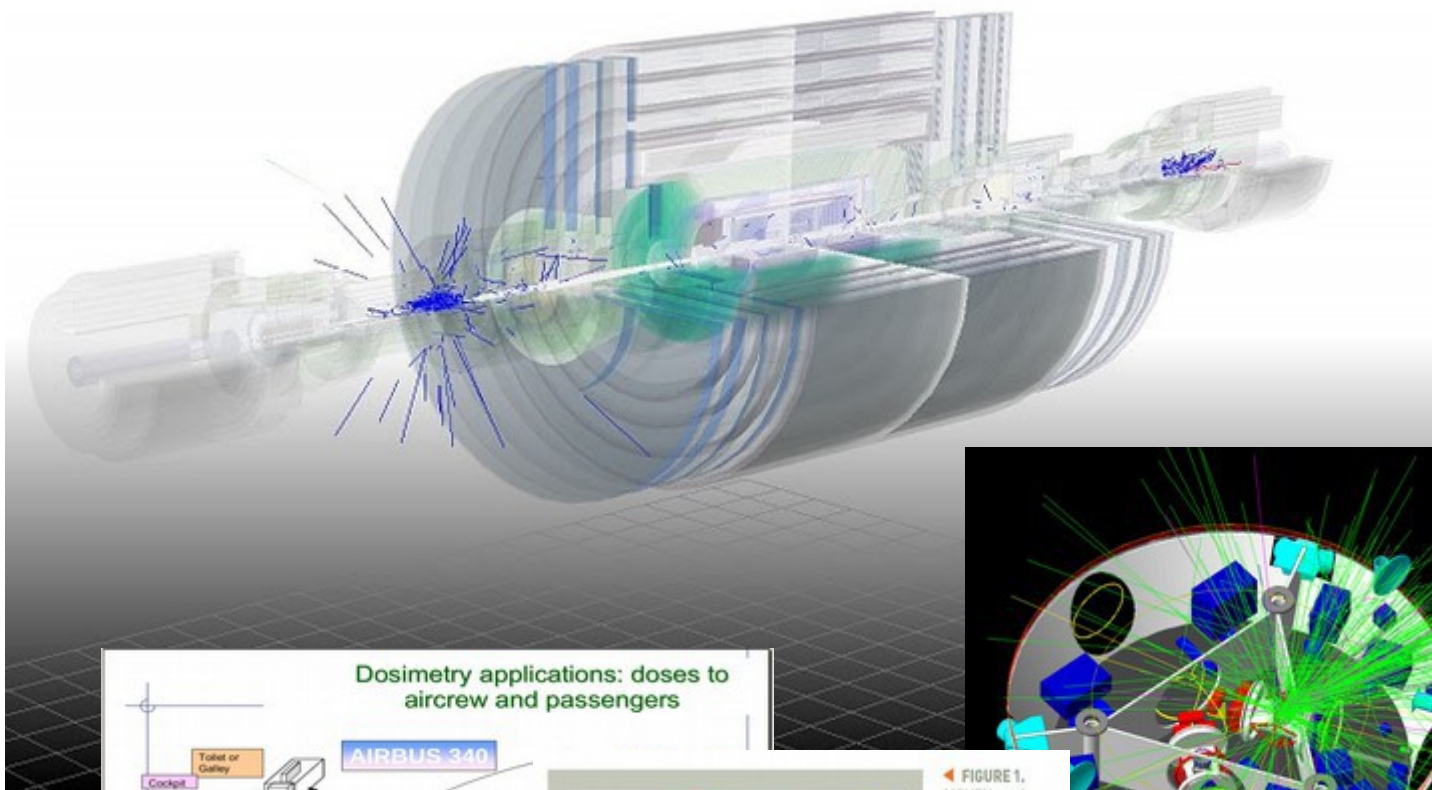
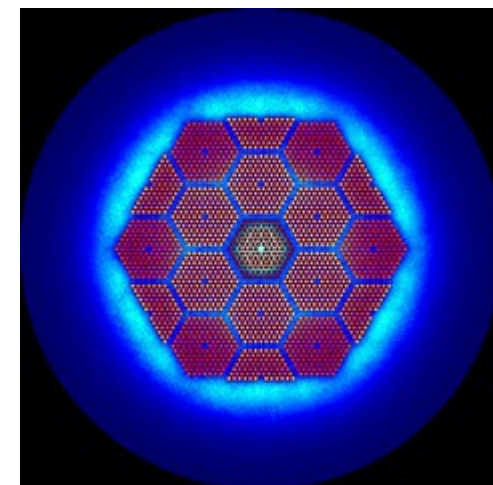
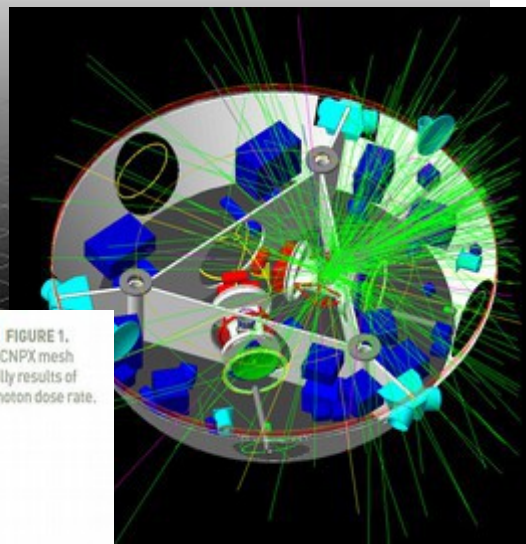
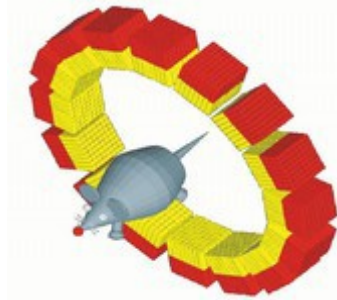
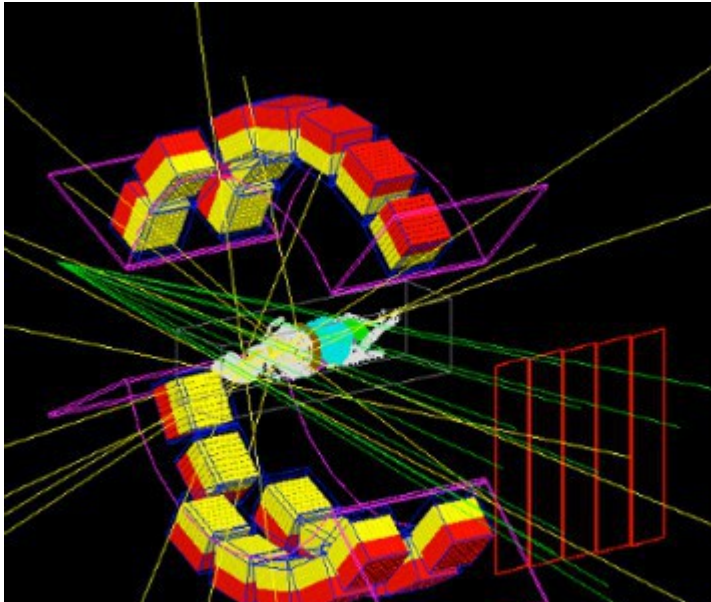


FIGURE 1. MCNPX mesh tally results of photon dose rate.

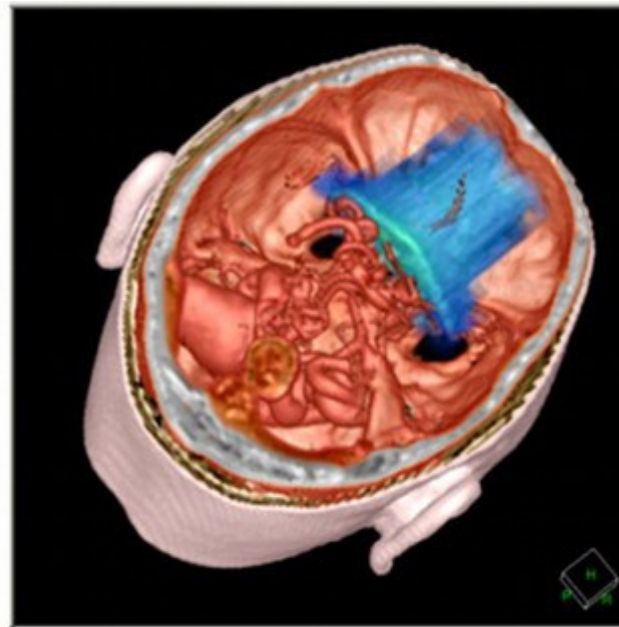
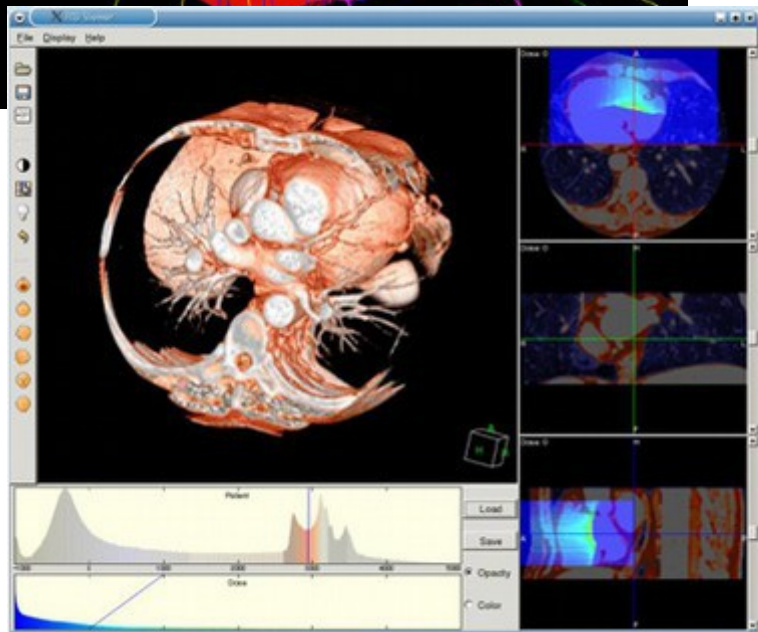


# Monte Carlo – Usage Examples



MEDICAL:  
PET/CT, Photons,  
electrons, ions therapy.

Dose/fluence spectra  
calculations





# Recommended Literature



Bielajews unfinished book on MC calculations:

<http://www-personal.umich.edu/~bielajew/DosimetryBook/book.pdf>

C-M Ma and Jinsheng Li 2011 Phys. Med. Biol. 56 3073

doi: 10.1088/0031-9155/56/10/012

## **Monte Carlo Treatment Planning An Introduction**

Report 16 of the Netherlands Commission on Radiation Dosimetry

go to <http://radiationdosimetry.org/ncs/documents/ncs-16->

